

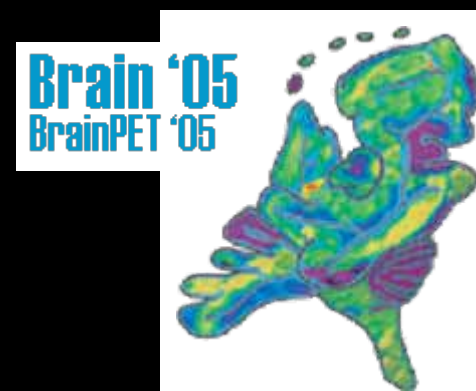
# Parametric Imaging of [ $^{11}\text{C}$ ]PIB Studies Using Spectral Analysis

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# Introduction

- [ $^{11}\text{C}$ ]PIB has previously been shown to be a marker of amyloid deposits in brain of Alzheimer's disease (AD) patients.
- Clinical question: Is a differential diagnosis of early dementia with imaging techniques possible?
- PET study design which is able to reliably distinguish between amyloid load in normal elderly, AD and other types of dementia is required.
- Because of the scattered occurrence of focal amyloid deposits in AD, exploratory interrogation of parametric binding images with statistical parametric mapping (SPM) may be more appropriate than an *a priori* defined region-of-interest based analysis.

## Focus of this presentation

**Comparison between different methods of quantification using arterial plasma input function with a view on the generation of parametric images.**

# Methods

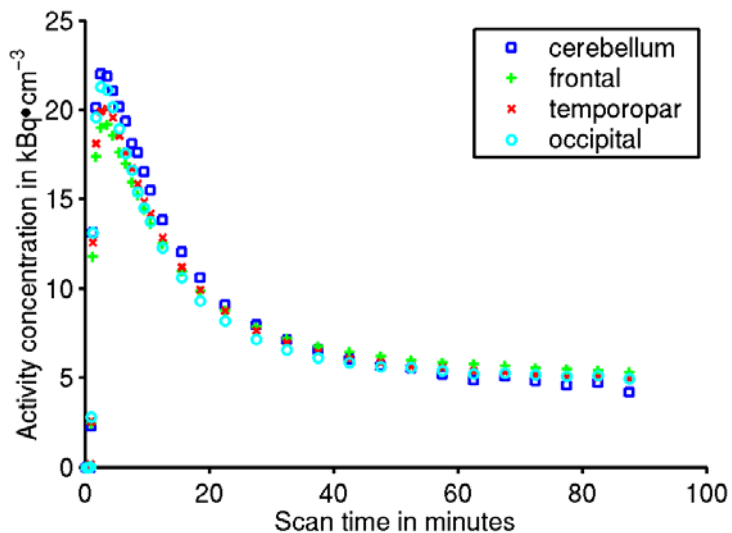
- Intravenous bolus administration of 370 MBq [<sup>11</sup>C]PIB.
- 3D dynamic PET data acquired for 90 min, ECAT EXACT HR+ scanner.
- Metabolite corrected arterial plasma input function using online blood detector and discrete arterial samples, metabolite analysis on HPLC system.
- Regions of interest (ROIs) were defined on T<sub>1</sub> weighted MR images coregistered with the PET images summed from 10 min to 90 min.
- Graphical analyses of reversible binding (Logan plot) and of irreversible binding (Patlak plot), assuming a fractional blood volume of 5 % and defining the linear part of the plot from 35 min onwards. Outcome measures:
  - \* the total volume of distribution from the Logan plot: **VD**,
  - \* the net accumulation rate constant from the Patlak plot: **K<sub>acc</sub>**.
- Spectral analysis with functions logarithmically spaced between  $\beta_{\min} = 0.0008 \text{ s}^{-1}$  ( $\log_{10} \beta_{\min} = -3.0969$ ) and  $\beta_{\max} = 0.1 \text{ s}^{-1}$  ( $\log_{10} \beta_{\max} = -1$ ). From the obtained set of  $n$  peaks in the spectra (peak position  $\beta_i$ , peak height  $\alpha_i$ ), the following expressions were calculated:

\* the impulse response function : 
$$\text{IRF}(t) = \sum_{i=1}^n \alpha_i \cdot e^{-(\beta_i - \lambda) \cdot t}$$
  
(corrected for radioactive decay),

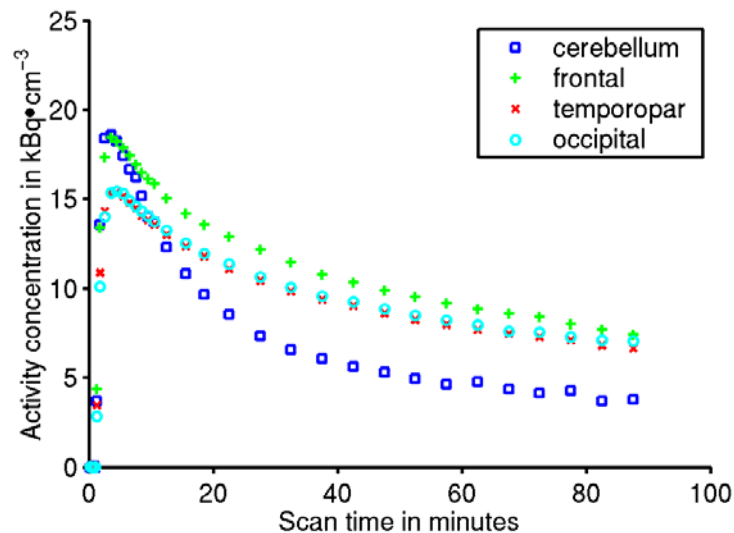
\* the volume of distribution (area under the curve of the IRF): 
$$\text{VD} = \sum_{i=1}^{n-1} \frac{\alpha_i}{\beta_i - \lambda}$$
  
(excluding the blood volume peak).

# Results: tissue time-activity curves

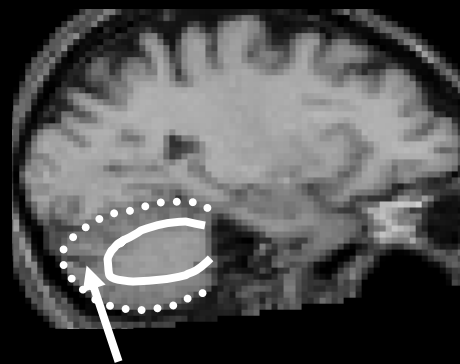
## Control subject



## Alzheimer's patient

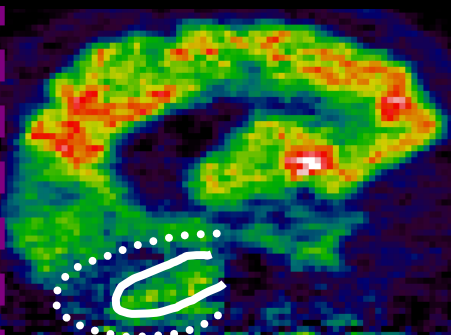
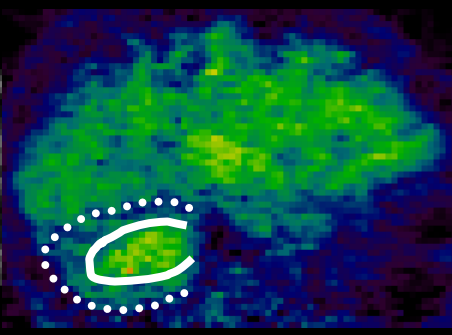


### MR image



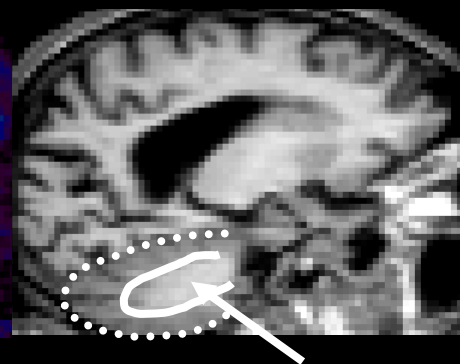
cerebellar grey matter

### sum images 10 ... 90 min



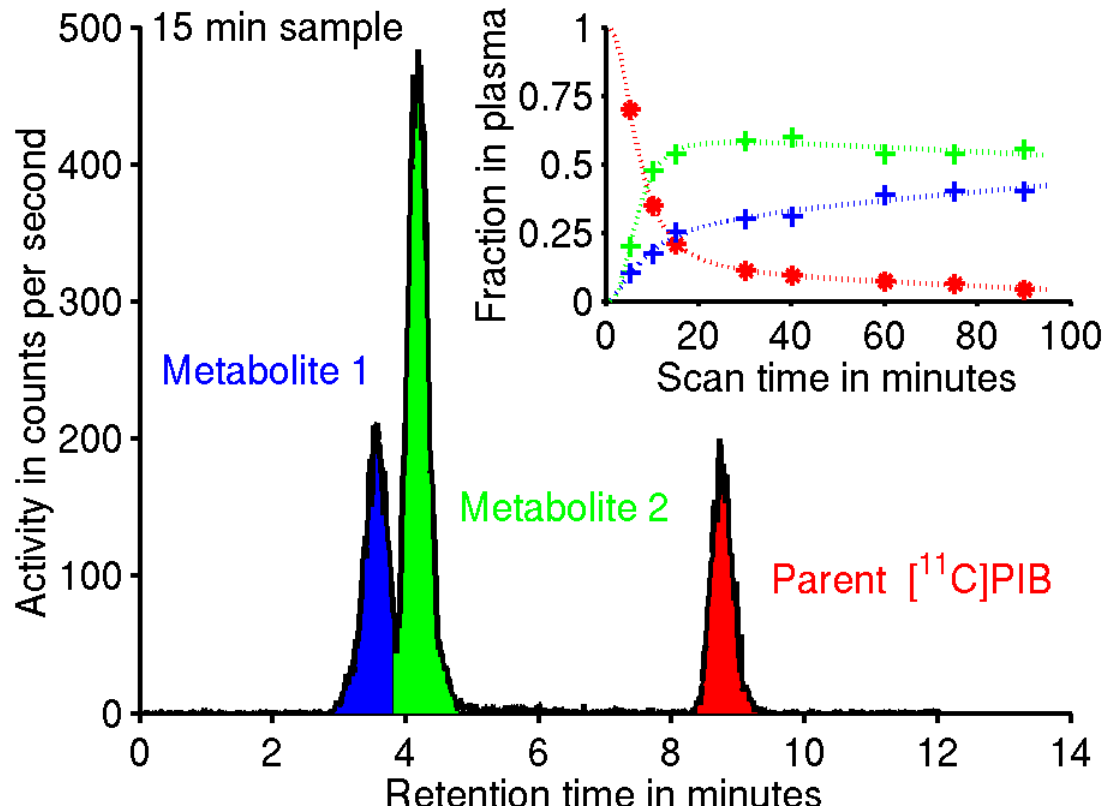
0  15  $\text{kBq}\cdot\text{cm}^{-3}$

### MR image



cerebellar white matter

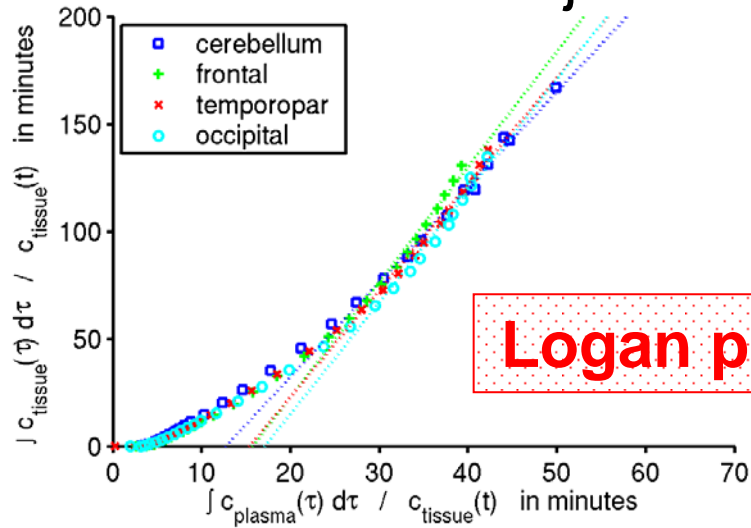
# Results: plasma input function



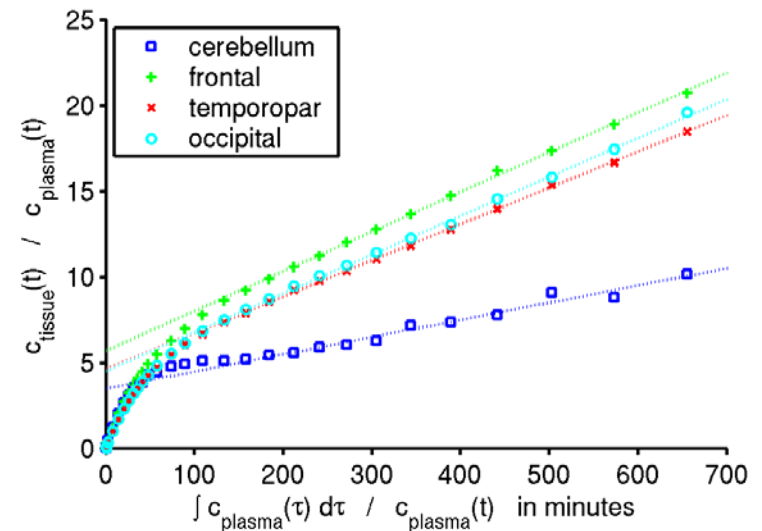
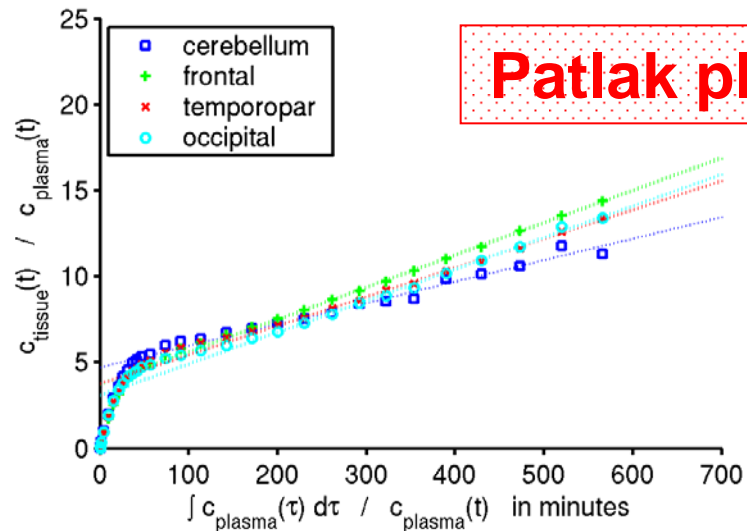
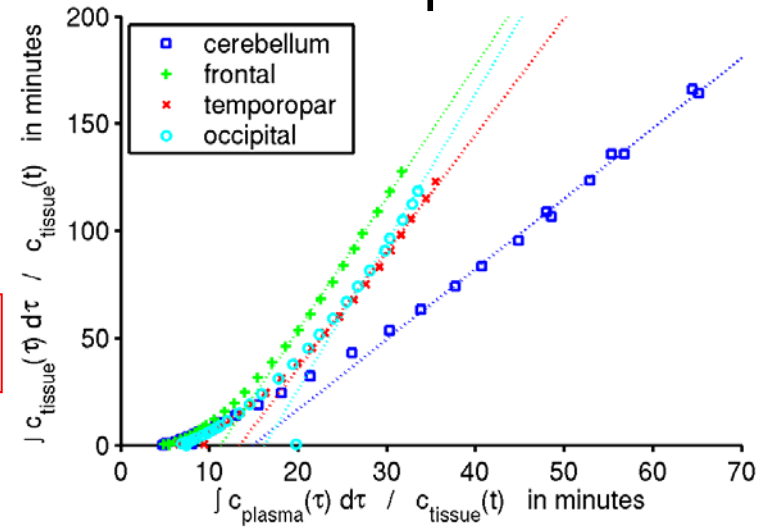
- No lipophilic metabolites were detected in the HPLC trace.
- The two metabolites 1 (blue) and 2 (green) have a considerably shorter retention time on the column than [<sup>11</sup>C]PIB and overlap partially.
- The parent [<sup>11</sup>C]PIB (red) is relatively rapidly metabolised.

# Results: graphical analyses

## Control subject




## Alzheimer's patient




# Results: graphical analyses

Region	Logan plot				Patlak plot			
	control		AD subject		control		AD subject	
parameter	slope		slope		slope		slope	
unit	VD	ratio	VD	ratio	$K_{acc}$	ratio	$K_{acc}$	ratio
	ml·ml <sup>-1</sup>		ml·ml <sup>-1</sup>		min <sup>-1</sup>		min <sup>-1</sup>	
cerebellum	4.43		3.28		0.0125		0.0100	
frontal	5.35	1.21	6.17	1.88	0.0188	1.50	0.0232	2.32
temporopar	4.95	1.12	5.43	1.66	0.0169	1.35	0.0211	2.11
occipital	5.18	1.17	6.90	2.10	0.0184	1.47	0.0227	2.27
mean		1.17		1.88		1.44		2.23



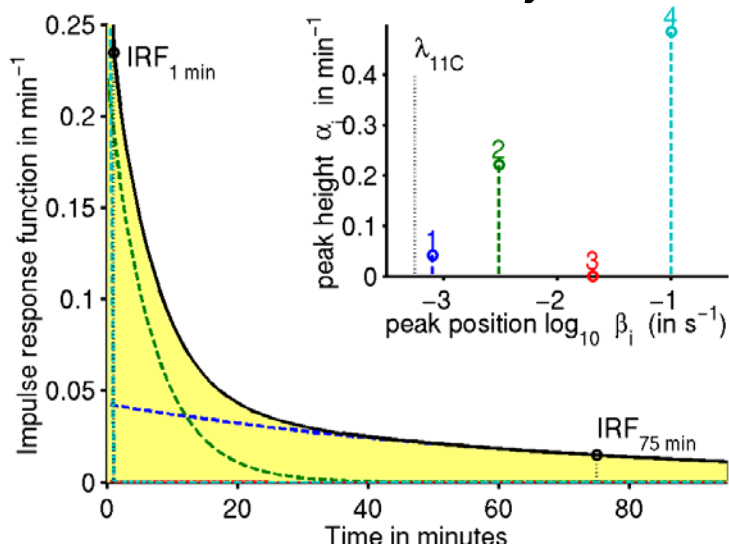
**61 % increase**



**55 % increase**

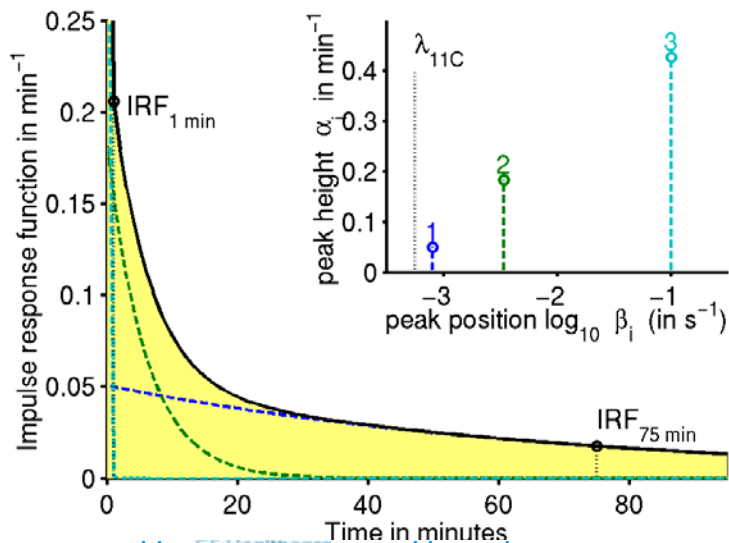
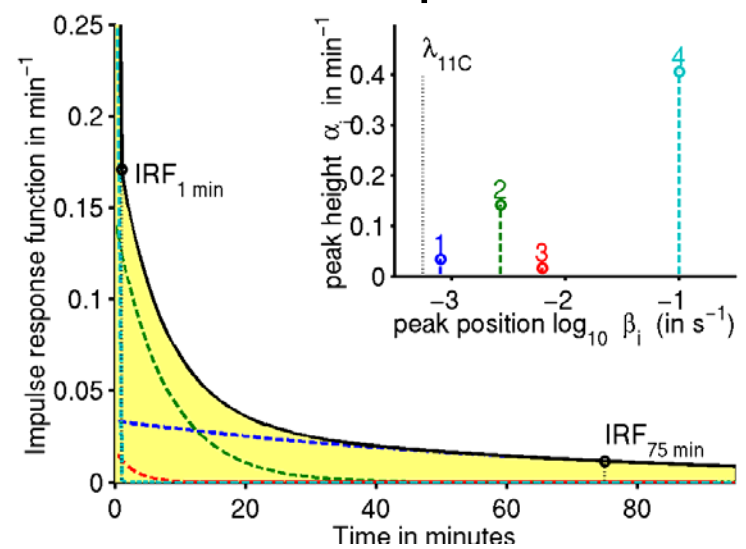
# Results: spectral analysis

Control subject

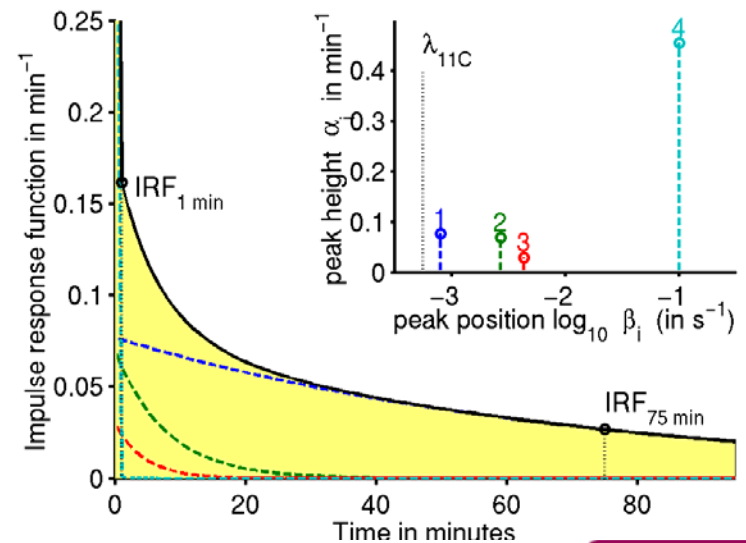


cerebellum

Alzheimer's patient




frontal





# Results: spectral analysis

		Spectral analysis					
Region		control		AD subject		contr.	AD
parameter		IRF <sub>75</sub>	ratio	IRF <sub>75</sub>	ratio	VD	VD
unit		min <sup>-1</sup>		min <sup>-1</sup>		ml·ml <sup>-1</sup>	ml·ml <sup>-1</sup>
cerebellum		0.0150		0.0117		4.53	3.54
frontal		0.0177	1.18	0.0268	2.28	4.70	6.14
temporopar		0.0161	1.08	0.0234	1.99	4.52	5.32
occipital		0.0156	1.04	0.0241	2.06	4.38	5.52
mean			1.11		2.11		

  
**90 % increase**

spectral analysis VDs are in agreement with Logan plot VDs

# Results: parametric images

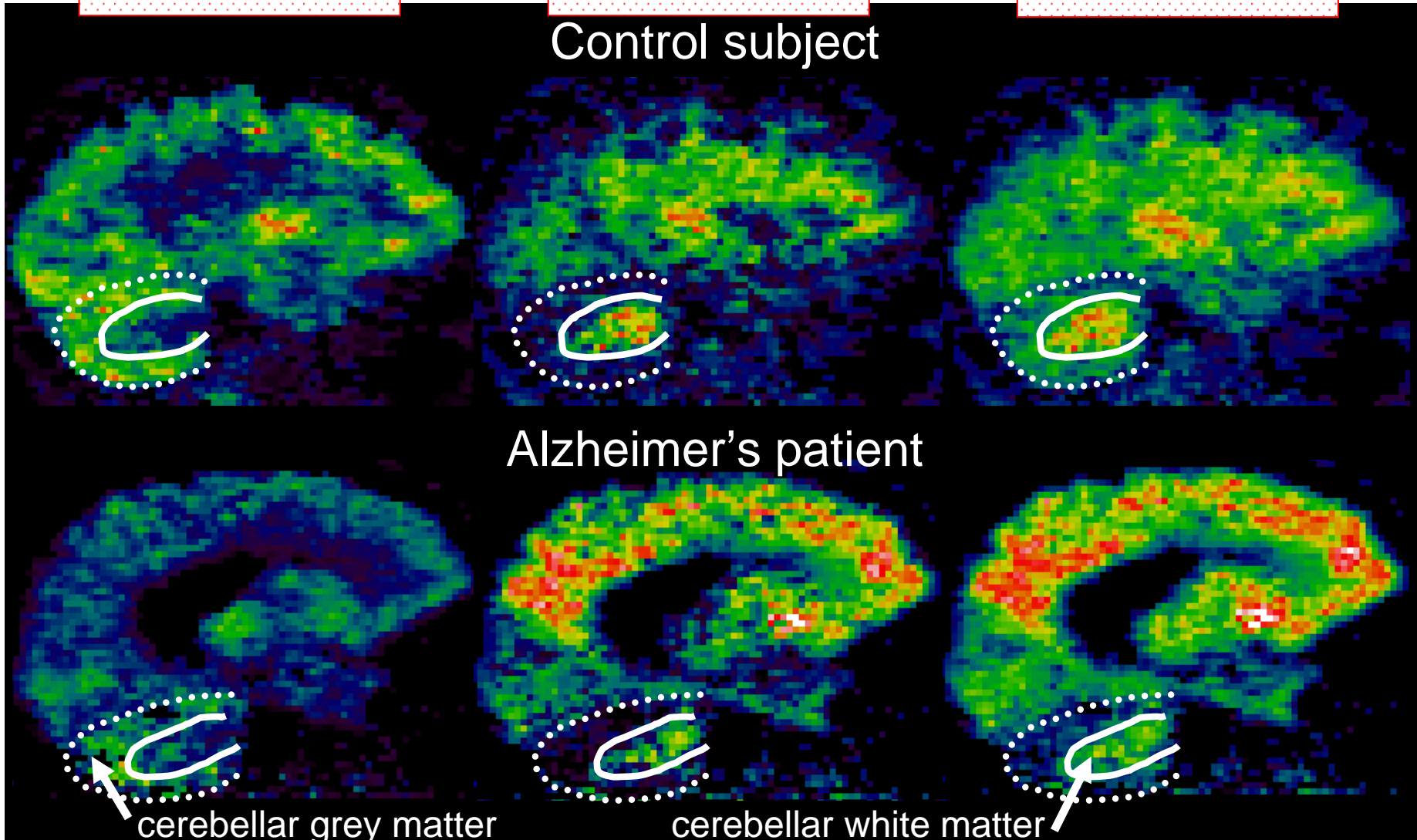
IRF 1min

IRF 75 min

VD

Control subject

Alzheimer's patient



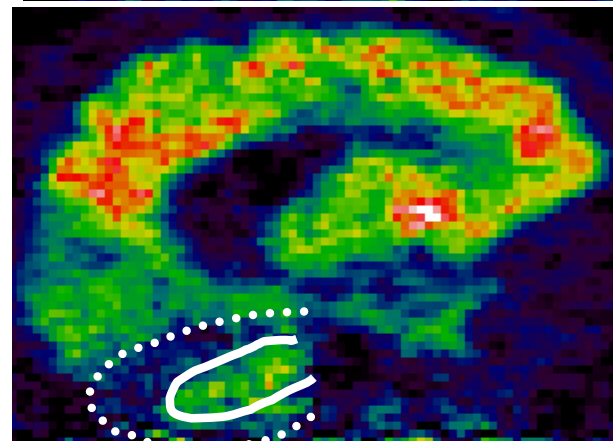
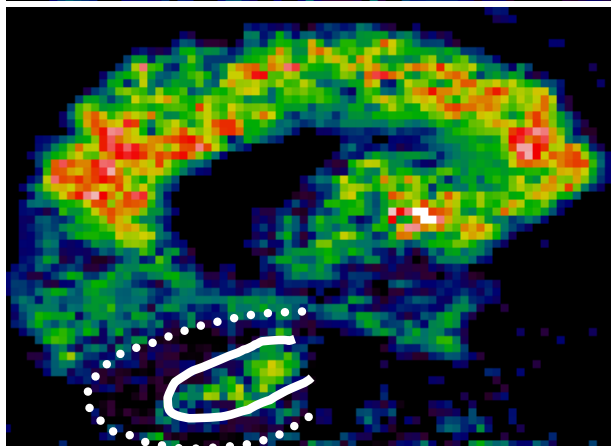
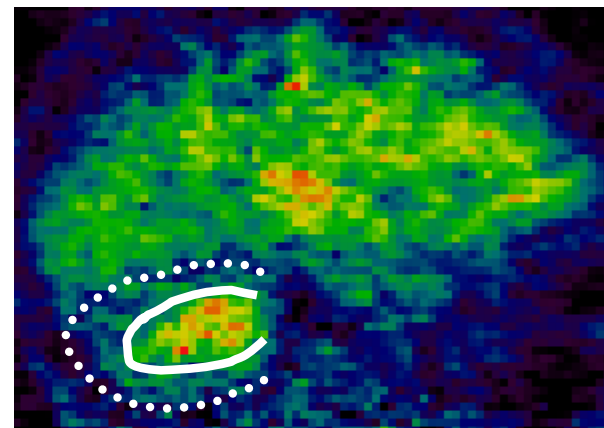
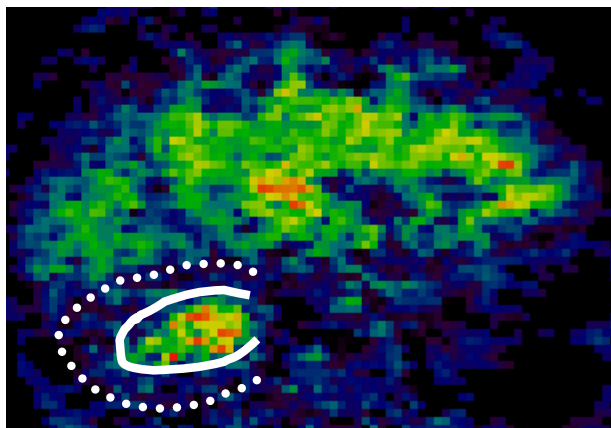
cerebellar grey matter

cerebellar white matter

# Results: parametric images

IRF 75 min

$$K_{\text{acc}} = \frac{K_1 \cdot k_3}{k_2 + k_3}$$



Control subject  
AD patient

See poster presentation BP-84: G. Blomquist et al.  
“Different patterns of PIB uptake in AD patients.”

# Conclusions

- Spectral analysis is a powerful tool for the generation of parametric images from [ $^{11}\text{C}$ ]PIB studies. It separates the tissue response function into the early, blood flow dependent signal component and the later signal component indicative of [ $^{11}\text{C}$ ]PIB retention to amyloid plaques.
- Imaging the IRF at late time produces a higher contrast than the VD image.
- The use of spectral analysis does, however, require the measurement of the plasma input function.
- Further work will include comparisons of reference tissue methods and whether shorter scan times are feasible.